

# Enhancing cardiac image segmentation through persistent homology regularization

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- 2 Cubical Complexes
- 3 Experiments
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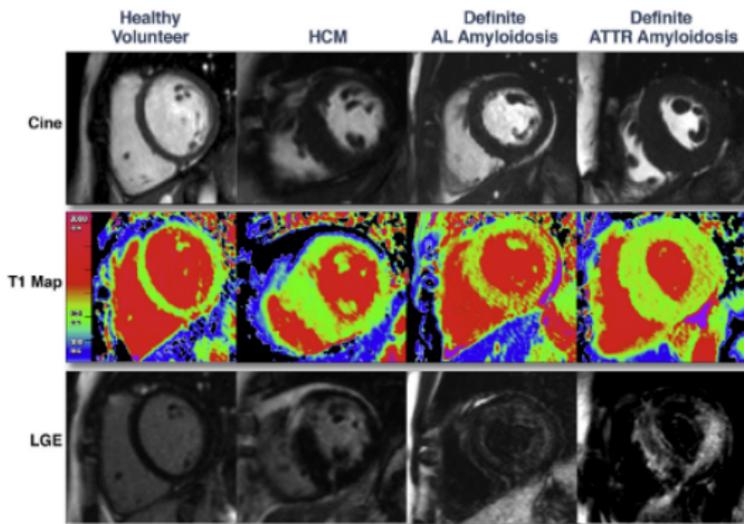
# Cardiac image segmentation

- Global impact of cardiovascular diseases (CVDs)
- Importance of early diagnosis in preventing CVDs
- The process of whole heart segmentation (WHS) and its significance in clinical applications

# Deep learning algorithms

- Recent advancements in machine learning models for cardiac magnetic resonance (CMR) image segmentation
- Need for extreme accuracy in cardiac image segmentation
- Rise of deep learning algorithms to improve accuracy

# Diagnosing diseases with deep learning



**Figure:** From top to bottom: CMR end-diastolic cine still, shortened modified look-locker inversion recovery native T1 map, and late gadolinium enhancement (LGE) images. From left to right: healthy volunteer, hypertrophic cardiomyopathy (HCM), definite immunoglobulin light-chain amyloidosis (AL amyloidosis), and definite transthyretin amyloidosis (ATTR amyloidosis) patients. Source of the image: *Fontana et al., 2014*

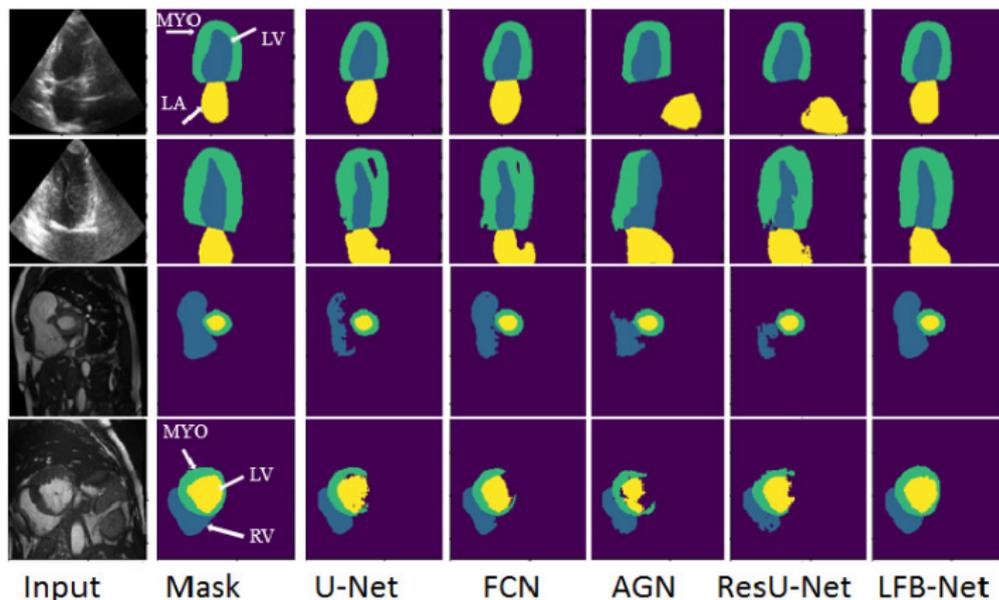
# Problems with deep learning CMR segmentation

- The complexity of the heart as a multi-element organ
- The difficulties in comparing different methods due to differences in datasets and evaluation metrics
- The limitations of using fully convolutional networks (FCNs) for heart segmentation

# Problems with deep learning CMR segmentation

- Benefits of incorporating prior knowledge in medical image analysis
- Improved accuracy of models with prior knowledge [Masoud et al., 2016]

# Topology priors in segmentation

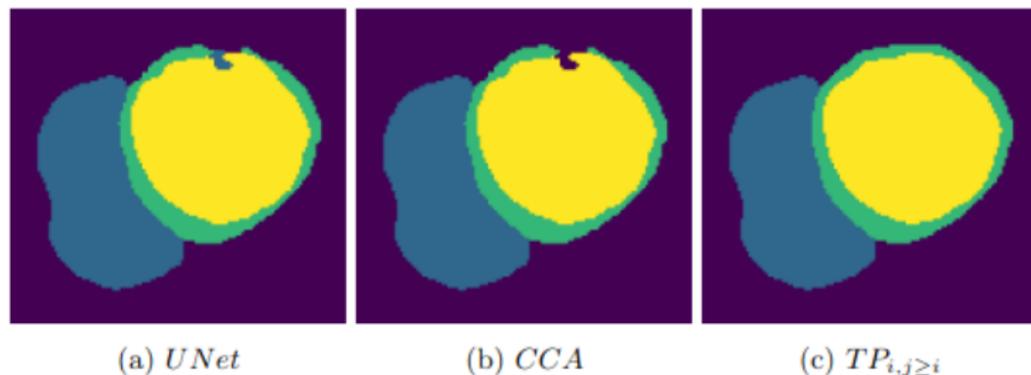


**Figure:** Examples of multi-label cardiac image segmentation results. [Rows 1-2] long-axis echocardiography and [Rows 3-4] short axis cine-MRI segmentation. RV: Right ventricular cavity; LV: Left ventricular cavity; MYO: Myocardium; and LA: Left atrium. Source of the image: *Berihu Girum et al., 2021*

The use of topology in cardiac image segmentation has several benefits:

- Topology can be used to identify and quantify the topological features of an object
- Topology can be used to track the progression of changes in the topological structure of an object over time
- Topological analysis exhibits robustness against noise

# Prior knowledge of topology in segmentation



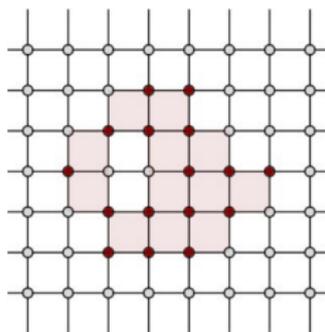
**Figure:** Topological post-processing enables expressive correction of U-Net and connected component analysis errors. Source of the image: *Clough et al., 2020*

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Cubical graphs are

- Useful when analyzing digital image data
- Located in a grid
- Sized fixed by the grid

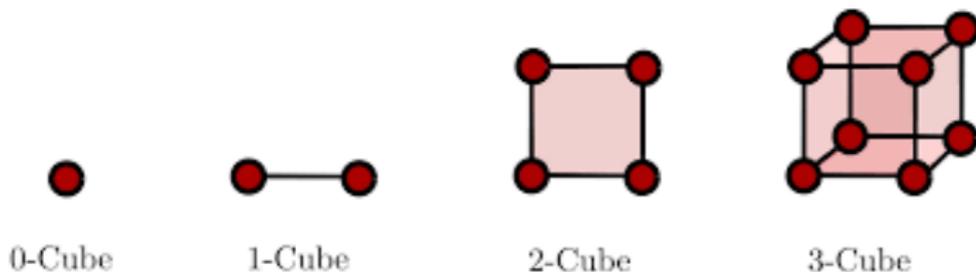


# Geometrical cubes

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We want a generalization of the concept of a square or a cube to any number of dimensions



- A 0-cube corresponds to a vertex
- A 1-cube corresponds to an edge
- A 2-cube corresponds to a square
- A 3-cube corresponds to a cube

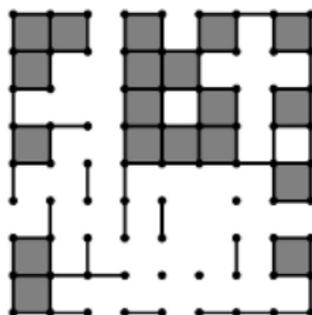
## Definition

A **cubical complex**  $K$  is a collection of  $n$ -cubes so that if  $c \in K$  and  $c' \subseteq c$ , then  $c' \in K$ .

# Cubical complexes

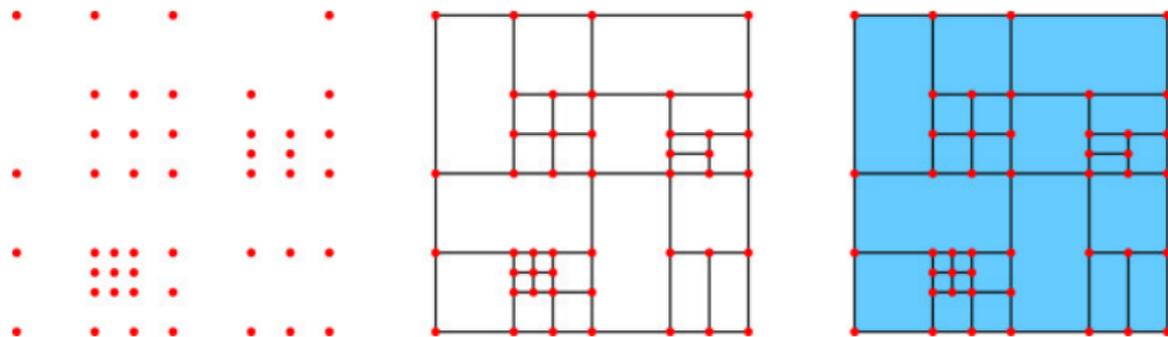
$$K = \{\text{vertices, edges, squares, } \dots\}$$

- $e \in K$ , with  $e$  an edge, then the vertices of the edge  $v_1, v_2 \in e$  will also be included in  $K$ .
- $s \in K$ , with  $s$  a square, then the vertices and edges of the square  $v_1, v_2, \dots \in s$  and  $e_1, e_2, \dots \in s$  will also be included in  $K$ .
- ...



## Definition

A **filtration** is a sequence of cubical complexes  $\{K_i\}_{i \in I}$  such that  $K_0 \subseteq \dots \subseteq K_n$ .



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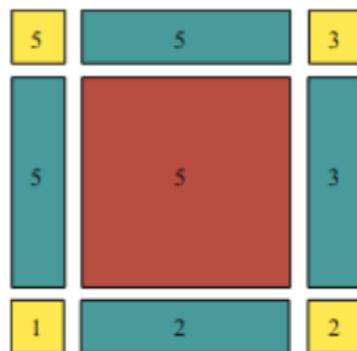
## Definition

Let  $K$  be a cubical complex. A real-valued function  $f: K \rightarrow \mathbb{R}$  is **monotonic** if  $f(\sigma) \leq f(\tau)$  when  $\sigma \subseteq \tau$ .

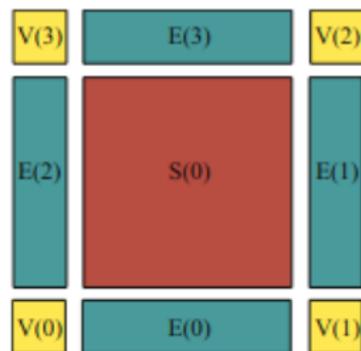
From monotonicity we derive that  $K(a) = f^{-1}(-\infty, a]$  is a subcomplex of  $K$  for every  $a \in \mathbb{R}$ . We call  $K(a)$  the **sublevel set** of the point  $a$ .

$$\dots \subseteq K(a_{i-2}) \subseteq K(a_{i-1}) \subseteq K(a_i) \subseteq K(a_{i+1}) \subseteq K(a_{i+2}) \subseteq \dots$$

- Lower-star filtration



(a)



(b)

# Persistence diagrams

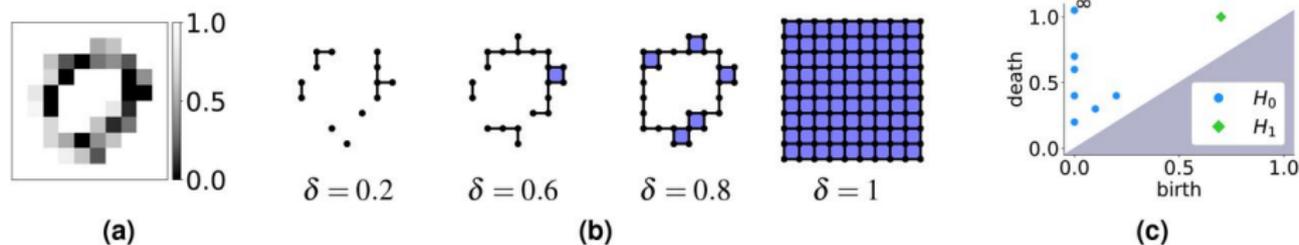
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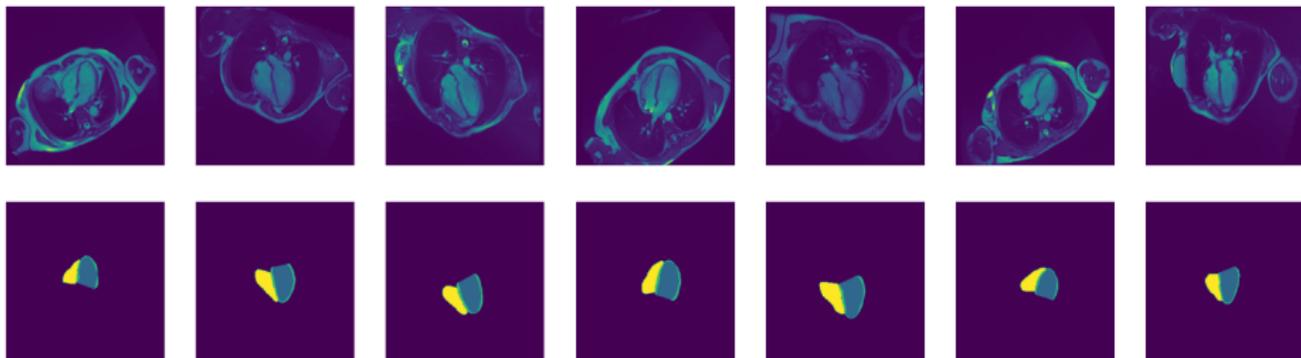
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## The dataset

- focuses on the right ventricle segmentation from CMR
- obtained from the second edition of the M&Ms Challenge [Campello et al., 2021]
- contains 360 CMR studies
- is divided in short-axis and long-axis 4-chamber views that are labeled at the end-diastolic (ED) and end-systolic (ES) phases



- 720 long-axis images
- Input images were rescaled to values in the interval  $[0,1]$
- Four channels were considered in the labels
- The selected input shape was  $128 \times 128 \times 1$
- The selected output shape of  $128 \times 128 \times 4$

# Neural network hyperparameters

# Neural network hyperparameters

Accuracy measures:

- **Categorical Cross Entropy Accuracy:**  $CE = - \sum_i^{N_{classes}} y_i \log(\hat{y}_i)$
- **Intersection-Over-Union:**  $IoU = \frac{|Y \cap \hat{Y}|}{|Y \cup \hat{Y}|}$
- **Dice Coefficient:**  $DC = \frac{2|Y \cap \hat{Y}|}{|Y| + |\hat{Y}|}$

Optimizer:

- The selected optimizer is **Adam**, with a learning rate of  $lr = 0.001$

# Cost function

Cost function:

$$\mathcal{L} = \mathcal{L}_{Dice}(Y, \hat{Y}) + \alpha \mathcal{L}_{Pixel-Wise}(Y, \hat{Y}) + \beta \mathcal{L}_{Regularizer}(Y, \hat{Y}),$$

$$\alpha = 2.0, \beta = 0.0025$$

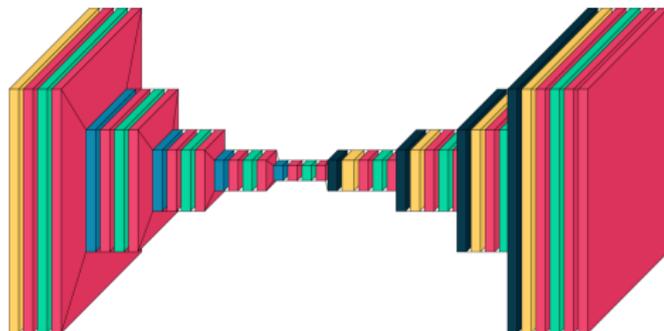
We used the following topological regularizers:

- Difference of total persistences
- Bottleneck distance

We employed topological regularizers to compare the deviation between the model's predictions and actual labels in segmentations of the right ventricle (RV), left ventricle (LV), and myocardium (MYO).

# Model

- The selected model is a **U-Net** neural network
- Input's data shape is  $128 \times 128 \times 1$
- Output's data shape is  $128 \times 128 \times 4$
- Convolution layers with  $2 \times 2$  and  $3 \times 3$  filters
- Dropouts of 10% and 20% of the neurons
- **RELU** activation function



**Figure:** 3-D visualization of the model's downsampling and upsampling paths.

The term **channel** refers to the segmentation of the right ventricle (0), left ventricle (1), myocardium (2), or background (3).

Losses:

- $GL := \text{Dice Loss} + \text{Pixel-Wise Loss}$
- $BL(\text{channel}) := \text{Bottleneck Loss applied to a specific channel for dimension 0 and 1. We have that } BL(\text{channel}) = \alpha(\text{bottleneck distance for dimension 0}) + \beta(\text{bottleneck distance for dimension 1}), \text{ with } \alpha = 1.1 \text{ and } \beta = 1.25.$
- $TP := \text{Difference of total persistences on all channels and dimensions}$

Accuracies:

- $CE := \text{Categorical Cross Entropy Accuracy}$
- $\text{MeanIoU} := \text{Intersection-Over-Union}$
- $DC := \text{Dice Coefficient}$

**Table:** Comparison of results of the combination of geometric losses without a topological regularizer vs results from the calculation of BL loss for each channel,  $i = 0, \dots, 3$ .

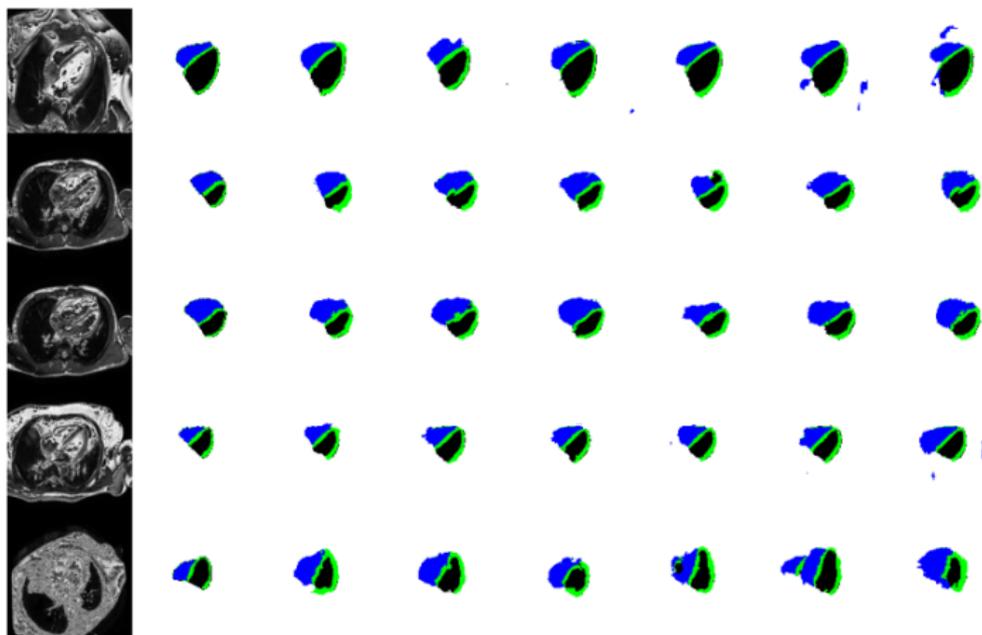
Metric	GL	GL+BL(0)	GL+BL(1)	GL+BL(2)	GL+BL(3)
MeanIoU accuracy (%)	61.0391	64.2347	66.0457	65.7243	63.1268
CE accuracy (%)	95.2583	96.1227	96.4405	96.3299	96.0592
DC accuracy (%)	96.2591	96.9546	97.1654	97.0742	96.8970

Losses:

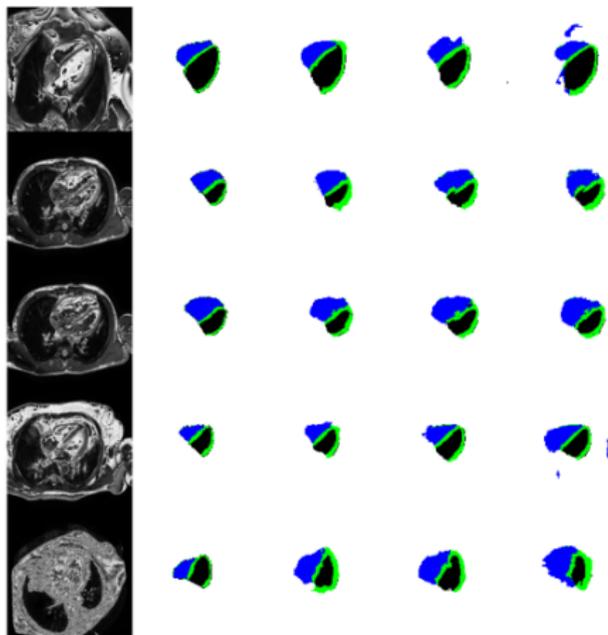
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**Figure:** Example of segmentations using different methods. From left to right: input images, labels, and segmentation methods BL(0)+GL, BL(1)+GL, BL(2)+GL, BL(3)+GL, TP+GL, and GL alone.



**Figure:** Example of segmentations using different methods. Left to right: input images, labels, and segmentation methods BL(0)+GL, BL(1)+GL, and GL.

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- We found promising results, indicating that the use of topological regularization did in fact lead to an improvement in segmentation accuracy
- However, there is still room for improvement in terms of the computational efficiency of these methods

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- Apply topological regularizers to a larger neural network using the whole dataset